

A Primer on Image Segmentation

It's all PDE's anyways

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- 1 Motivation
- 2 Simple Methods
- 3 Edge Methods
- 4 PDE Energy Methods
- 5 Other Methods
- 6 Parting Thoughts

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Real-World Problem

Develop new treatments for tuberculosis (*Mycobacterium tuberculosis*)

- $\approx 1/3$ of global population currently infected
- most common infectious disease worldwide
- 2 phases: innate immune response, then dormancy
- Factors in the transition between these phases only partially known

Goal: Track Mtb within infected cells during innate immune response

Real-World Problem

MTB Movie

Other Motivations

- Computer vision
- Self-driving cars
- Medical imaging (MRI, CT, ultrasound)
- Fingerprint recognition
- Art history and restoration

Some Notation

- Ω image domain, normally $[0, 1]^2$ or $[0, 1]^3$
- $u_0 : \Omega \rightarrow [0, 1]$ greyscale image
- $\Gamma \subset \Omega$ desired segment

Implemented in OpenCV + FEniCS in Python

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Simple Methods

Why?

- fast
- intuitive

When?

- no noise, blurring, obstructions, or known already
- know some properties already

Sweatshop Method

- robust to noise, blurring, variable contrast, halo effects
- often treated as "best possible" or ground truth
- time-consuming
- reliable?

Thresholding

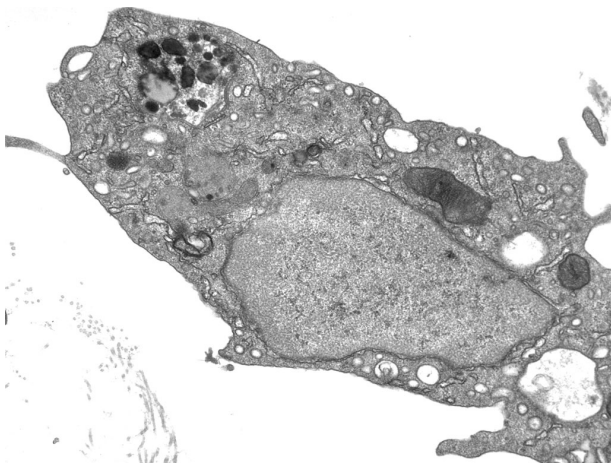
For a given threshold θ ,

$$\Gamma = \mathbf{1}_{\{u_0(x) \geq \theta : x \in \Omega\}}$$

Works best when

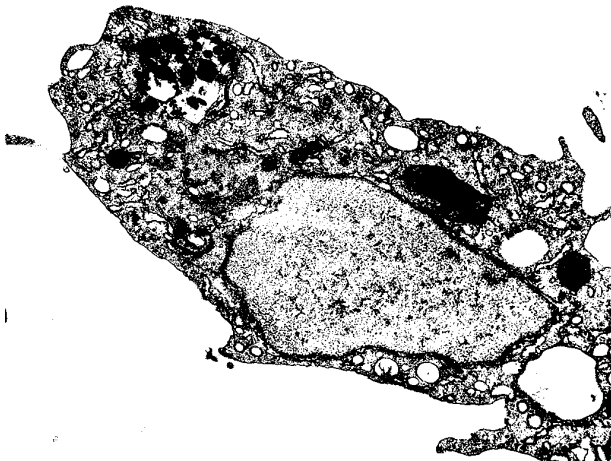
- clear foreground + background
- items to segment have similar intensities
- no variable contrast, obstructions

Thresholding



A macrophage

Thresholding



A macrophage, thresholded

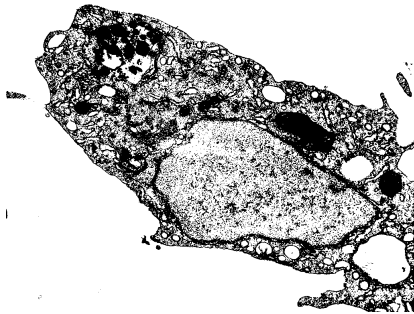
Local Thresholding

For a given threshold **map** $\theta : \Omega \rightarrow [0, 1]$,

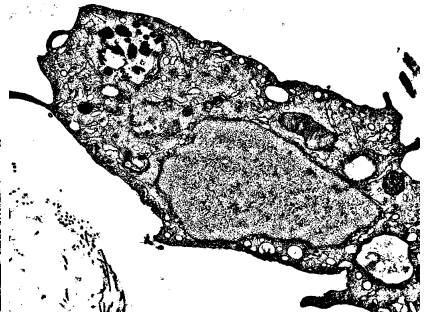
$$\Gamma = \mathbf{1}_{\{u_0(x) \geq \theta(x) : x \in \Omega\}}$$

For example, $\theta(x) = \text{average}\{u_0(y) : y \in B_\epsilon(x)\}$

Local Thresholding



(a) Thresholding



(b) Local Thresholding

Simple Methods can Fail

Problems when...

- noise
- blurred or obstructed objects
- halo / variable contrast or lighting
- no prior assumptions on object shape

Simple Methods can Fail



Cow!

Simple Methods can Fail



Cow: Thresholding

Simple Methods can Fail



Cow: Adaptive Thresholding

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Edge Detection

Motivation: Define edges as areas across high gradients

Interior within edges gives us segmented region Γ
→ can recover with e.g. watershed algorithm

Canny Edge Detection

- Given image u_0
- Apply smoother (e.g. Gaussian kernel, Laplacian) $u_0 \mapsto u$
- Approximate ∇u by Finite Differences

$$\nabla u(x, y) = \frac{1}{h} \begin{bmatrix} u(x^+, y) - u(x, y) \\ u(x, y^+) - u(x, y) \end{bmatrix}$$

- Threshold $\|\nabla u\|$

Edge Detection



Not a Duck

Edge Detection



Canny Edges of a non-duck

Eikonal Equation

First order fully nonlinear PDE:

$$\begin{aligned}\|\nabla u\| &= 1 && \text{on } \Omega \\ u &= 0 && \text{on } \partial\Omega\end{aligned}$$

u : minimal distance to boundary over a uniform cost field
→ continuous version of Shortest Path

Eikonal Equation for Segmentation

Let $F = \text{CannyEdge}(u_0)$; solve

$$\begin{aligned}\|\nabla u\| &= \frac{1}{F} && \text{on } \Omega \\ u &= 0 && \text{on } \partial\Omega\end{aligned}$$

cost field \sim penalize crossing edges

Eikonal Equation: Numerical Solution

Numerical solution: Fast Marching Method

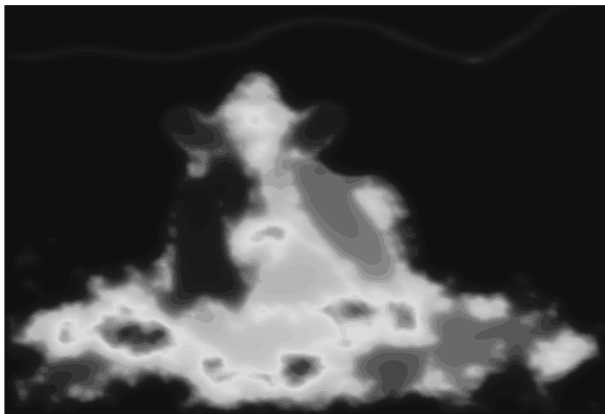
- Keep track of distance values for 'far', 'considered', 'accepted' nodes
- Update far nodes if accepted/considered nodes nearby → considered
- Considered with smallest value → accepted
- Repeat until no more considered nodes

Eikonal Equation: Fast Marching Method

Generalization of Dijkstra's algorithm

- more than just one previous node to calculate distance
- $O(\text{pixels}) = O(|V|) = O(|E|)$ runtime
Dijkstra's algorithm with integer weights on undirected graph

Eikonal Equation



Eikonal Equation



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Image Approximation

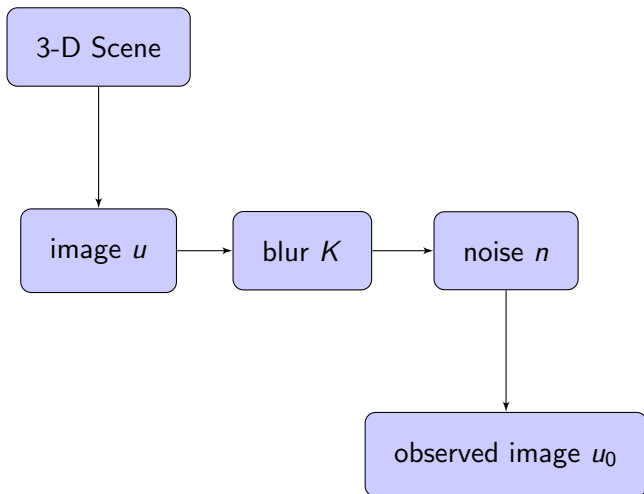


Image Approximation

Approximate $u_0 : \Omega \rightarrow [0, 1]$ by $u \in V$ vector space (often $H^1(\Omega)$)

Assumptions:

- well-defined solution space
- curvature of edges well-defined
- no fractals

Image Approximation with PDE Functionals

Goal: Define an energy functional on an image, then minimize functional

$$\hat{u} = \min_{u \in V, \Gamma \subseteq \Omega} E[u, \Gamma | u_0]$$

- Mumford-Shah
- Chan-Vese
- Ambrosio-Tortorelli

Mumford-Shah Functional

$$E[u, \Gamma | u_0] = \alpha \nu(\Gamma) + \frac{\beta}{2} \int_{\Omega \setminus \Gamma} |\nabla u|^2 dx + \frac{\lambda}{2} \int_{\Omega} (K[u] - u_0)^2 dx$$

- u_0 : image
- u : desired approximation
- $\Gamma \subset \Omega$: segmented section

Mumford-Shah Functional

$$E[u, \Gamma | u_0] = \alpha \nu(\Gamma) + \frac{\beta}{2} \int_{\Omega \setminus \Gamma} |\nabla u|^2 dx + \frac{\lambda}{2} \int_{\Omega} (K[u] - u_0)^2 dx$$

- $\nu(\Gamma)$: (Hausdorff) length of curve $\partial\Gamma$
- Keeps from making a curve around every pixel

Mumford-Shah Functional

$$E[u, \Gamma | u_0] = \alpha \nu(\Gamma) + \frac{\beta}{2} \int_{\Omega \setminus \Gamma} |\nabla u|^2 dx + \frac{\lambda}{2} \int_{\Omega} (K[u] - u_0)^2 dx$$

- penalize regions of high gradient or crossing $\partial\Gamma$
- groups similar parts of the image into contiguous segments

Mumford-Shah Functional

$$E[u, \Gamma | u_0] = \alpha \nu(\Gamma) + \frac{\beta}{2} \int_{\Omega \setminus \Gamma} |\nabla u|^2 dx + \frac{\lambda}{2} \int_{\Omega} (K[u] - u_0)^2 dx$$

- keep u_0 close to u
- K image (deblurring) operator; often $K = I$

Mumford-Shah Functional

- Maintains edges in Γ while smoothing noise
- Use u instead of u_0 for other segmentation methods
- $V = \{ \text{piecewise constants} \} \rightarrow \text{thresholding}$

Mumford-Shah Functional



Still not a duck. . .

Mumford-Shah Functional

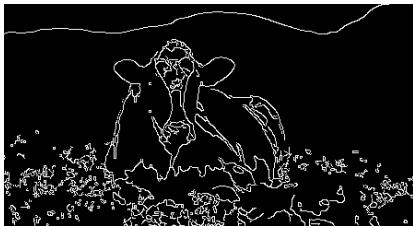


Mumford-Shah approximation of Cow

Mumford-Shah Functional



(a) Canny Edge on u_0



(b) Canny Edge on $u = MS[u_0]$

Mumford-Shah Functional

$$E[u, \Gamma | u_0] = \alpha \nu(\Gamma) + \frac{\beta}{2} \int_{\Omega \setminus \Gamma} |\nabla u|^2 dx + \frac{\lambda}{2} \int_{\Omega} (K[u] - u_0)^2 dx$$

- $\alpha, \beta, \lambda \geq 0$
- Chan-Vese Active Contour model: $\beta \rightarrow \infty$
- Ambrosio-Tortorelli: replace Γ region with Φ

$$x \in \Gamma \iff \Phi(x) \text{ large}$$

- Bilevel optimization problem

$$\hat{u} = \min_{\alpha, \beta, \lambda} \min_{u \in V} E[u, \Gamma | u_0]$$

Laplacian Models

Send $\alpha \rightarrow \infty$ and drop Γ dependence:

$$E[u|u_0] = \frac{\beta}{2} \int_{\Omega} |\nabla u|^2 dx + \frac{\lambda}{2} (K[u] - u_0)^2 dx$$

Theorem (Elliptic Solution)

Suppose $u_0 \in L^\infty(\Omega)$. Then, the energy functional $E[u|u_0]$ has a unique minimizer $u_ \in H^1(\Omega)$ that satisfies the elliptic PDE*

$$\begin{aligned} -\beta \Delta u + \lambda(u - u_0) &= 0 && \text{on } \Omega \\ \partial_n u &= 0 && \text{on } \partial\Omega \end{aligned}$$

Laplacian Models

Solve the following PDE:

$$\begin{aligned} -\beta \Delta u + \lambda(u - u_0) &= 0 && \text{on } \Omega \\ \partial_n u &= 0 && \text{on } \partial\Omega \end{aligned}$$

Multigrid solver \rightarrow resolution at different scales

- Hierarchical scale separation of image features
- Corner identification
- Skeleton construction (stick figures)

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Other Methods: Graphs

- min-cut
- normalized min-cut
- spectral Graph Laplacian
- equivalence to Finite Differences for specific PDE methods

Often have good algorithms!

Other Methods: Neural Networks

- CNN, U-Net
- Many different architectures
- Labeled training data
- Viewed as state-of-the-art

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Parting Thoughts

- Simple methods for occasional users
- PDE methods
 - PDEs provide strong analytical framework
 - Can be fast
 - robust to noise
 - Can do more complicated tasks: inpainting, deblurring, etc.
- Other methods
 - Graph methods
 - NN methods
 - need training data
 - hard analysis?
 - Scattering, Sampling, many others too!

Questions Moving Forward

- Extension to 3D?
- Learning on images, not just segmentation
- Incorporation into models
- Automation? Supervised? Semisupervised?
- Future Work:
 - Using PDE methods to evaluate NN fitness
 - Unrolling methods: bilevel optimization \mapsto NN